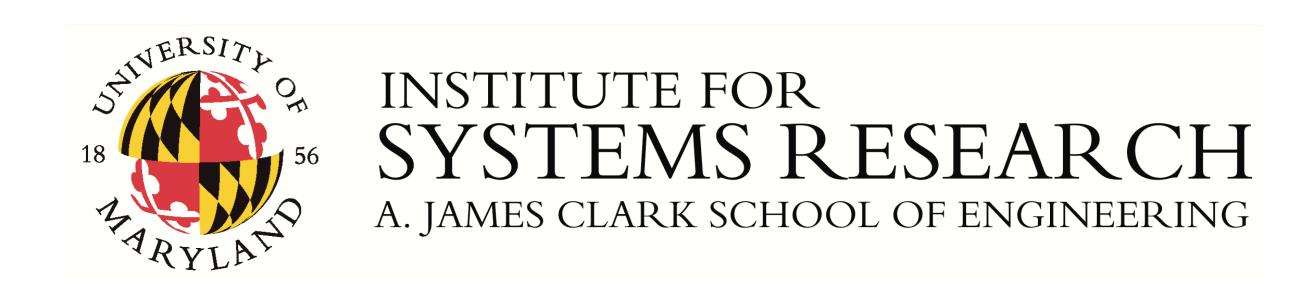
Efficient Sensing in Biosystems

Nicola Bertoni⁴, Fabio Pareschi⁴, Mauro Mangia³, Jonathan Z. Simon¹, Riccardo Rovatti³, Gianluca Setti^{3,4} Timir Datta-Chaudhuri¹, Bathiya Senevirathna¹, Alexander Castro¹, Elisabeth Smela², Pamela Abshire¹



¹Dept. of Electrical & Computer Engineering & ISR ²Dept. of Mechanical Engineering & ISR ³DEI, University of Bologna, Italy ⁴ENDIF, University of Ferrara, Italy

Event-Based Readout in Lab-on-CMOS: Spike Processing

Introduction

Sampling bio-potential data yields a large amount of data, however the actual information content of the signals is much sparser than the data being collected.

- Transient waveforms require high sampling
- 40 kSamples/s x 16 b/Sample x 32 channels → 154 MB/min
- Spike information is quite sparse: $< 100 \text{ Spikes/s } \times 32 \text{ channels } \rightarrow < 3.75 \text{ kB/}$ min

Instead of reading out the raw data by itself, we can match the asynchronous signal source with an event-driven readout

- This requires local spike detection capability
- Bandwidth requirements are reduced by a factor of 1600

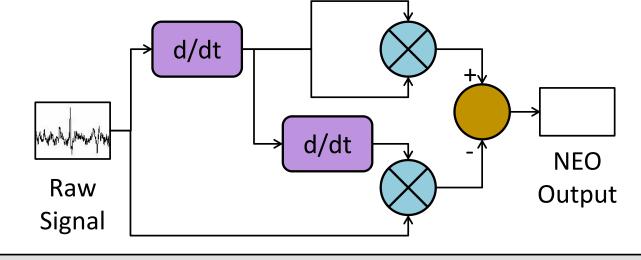
Circuit Implementation

NEO requires three fundamental computations: • Derivative: Input capacitor preceding a high-gain inverting

• Multiplier: Translinear four quadrant multiplier with core voltage loop created by six PMOS transistors

amplifier with resistive feedback

• Subtraction: Current-mode subtractor

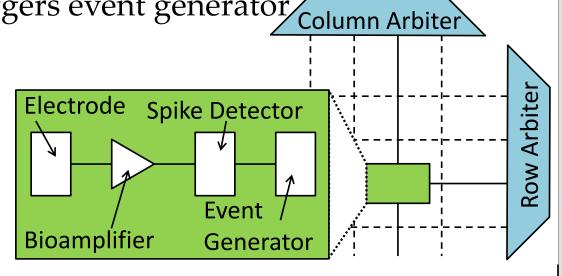


System Overview Electrode Array

- The system is an active micro-electrode array Array of sensor pixels
- Pixel: Electrode pair, bioamplifier, spike detection circuit, and Address Event Representation (AER) interface
 - Bioamplifier: Operational Transconductance Amplifier (OTA): $A_v = C_{in}/C_{fb} = 46 \text{ dB}$, $C_{in} = 20 \text{ pF}$, $C_{fb} =$ 100 fF, Passband: 280 mHz to 8.1 kHz
 - Spike Detector: Nonlinear Energy Operator (NEO) algorithm
 - **AER**: Asynchronous readout with full handshaking or autonomous self-timing operation
- Digital pulses sent off-chip to external Data Acquisition system (DAQ)

AER Protocol

- Spike detector triggers event generator Column Arbiter • Row and column
- arbitration controls address generation
- Single spatial address per spike event



Bandwidth Reduction Factor[†] (BRF) With typical data acquisition scheme:

 $40 \text{ kSamples/s} \times 16 \text{ b/Sample} \times 1 \text{ B/8 b} = 80 \text{ kB/s}$ With asynchronous readout:

 $50 \text{ AP/s} \times 8 \text{ b/AP} \times 1 \text{ B/8} \text{ b} = 50 \text{ B/s}$

per channel in a 16 channel system

Statistical Bandwidth Reduction: Compressed EEG Sensing

Introduction

The study of brain diseases such as schizophrenia has traditionally been performed using laboratory-based EEG and MEG devices. Wireless mobile sensing platforms can be a valuable tool in studying EEG patterns:

- Recording responses that are uncontrolled (e.g. hallucinations)
- Facilitates patient comfort

Problem:

• Battery lifetime: system should run continuously throughout the day

Proposed Solution:

• Compress EEG signals prior to data transmission in a computationally-simple manner

Low Cost Mobile EEG

Built from commercial-of-the-shelf components and facilitates on-board compressive sensing.

- Biopotential ADC: TI ADS1299
- High performance microcontroller: Atmel SAM G55
- Up to 7 EEG channels and one audio envelope channel

Environmental Noise Shaping

Hz environmental noise

- Up to 500 samples/s
- Bluetooth connectivity
- Low cost (\$200)

Compressed Sensing

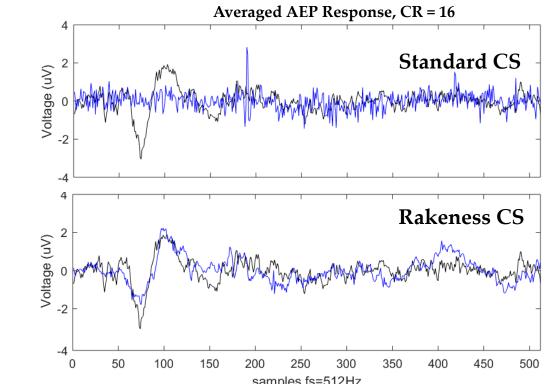
Compressive sensing (CS) is a technique of compressing acquired signals in real-time and in a low-power manner.

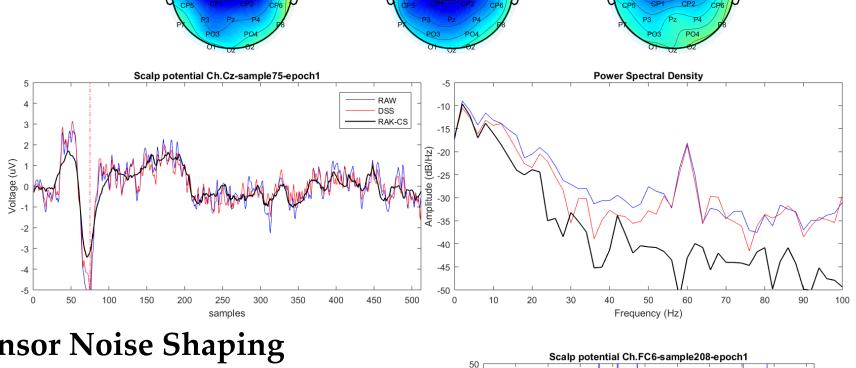
- Move bulk of computational effort in compression away from the battery-powered wireless node to a base station.
- Compression algorithm is designed to be simple (i.e. made of a few elementary operations)
- Decompression algorithm is inherently non-linear and usually more time- and energy-consuming.

Rakeness CS

Statistical tuning of the CS algorithm to the EEG signals of interest, resulting in implicit signal filtering

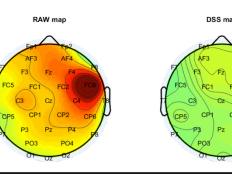
- Matched features are enhanced
- Other sources like noise are attenuated





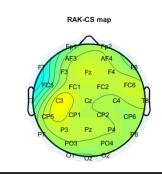
Tune Rakeness CS algorithm to filter out 60

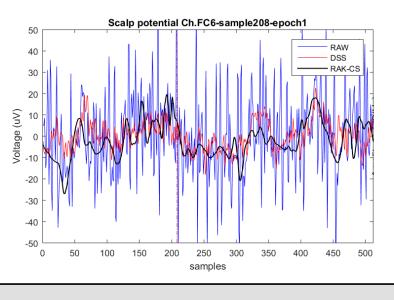
Sensor Noise Shaping Unwanted sensor motion filtered using Rakeness CS



Power Measurements

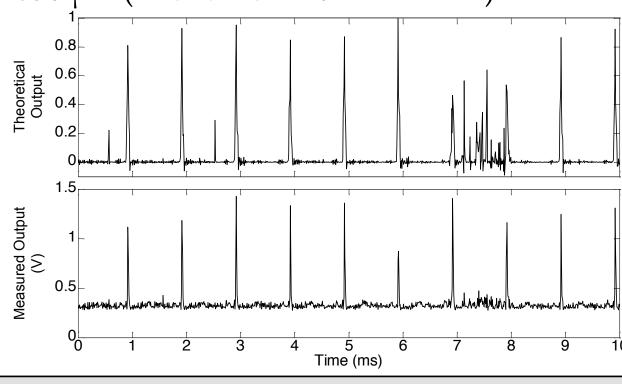
Power consumption of the mobile EEG system was measured as a function of the compression ratio and number



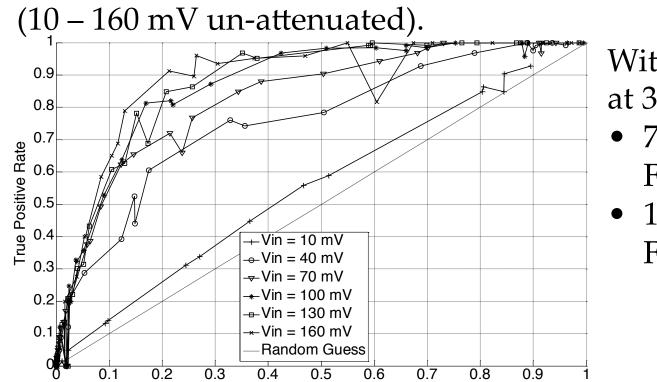


Experimental Verification

by providing a 1 kHz spike train with amplitudes of 850 μ V (attenuated from 12.7 mV).



Computational accuracy of NEO circuit measured Receiver operating characteristic showing detection rate (DR) vs. false positive rate (FPR). Spike amplitudes of $55 - 900 \mu V$



With input spikes at 390 μV:

• 76% DR vs. 5% • 100% DR vs. 14%

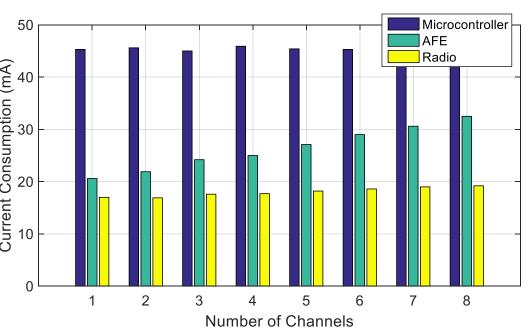
BRF:

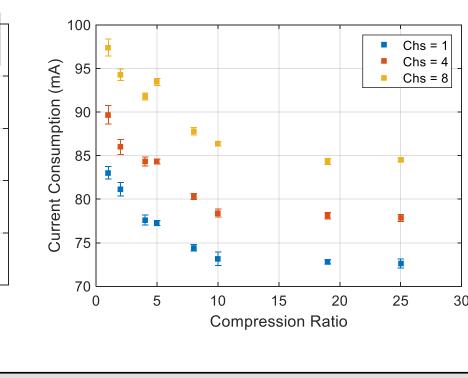
1600

of EEG channels being recorded • Diminishing returns as compression ratio is increased

• AFE contributes most to increase in power consumption as more channels are added (58% increase in consumption vs. 13% increase)

 Microcontroller processing cost was negligible compared to overhead











Phase II STTR award #FA8651-14-C-0107

UMD Engineering **Systems for Medicine**

